The pH Low Insertion Peptide pHLIP Variant 3 as a Novel Marker of Acidic Malignant Lesions

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The pH low insertion peptide pHLIP Variant 3 as a novel marker of acidic malignant lesions

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Contributed by Donald M. Engelman, May 29, 2015 (sent for review January 20, 2015; reviewed by Lin Z. Li and Avraham Raz)

Current strategies for early detection of breast and other cancers are limited in part because some lesions identified as potentially malignant do not develop into aggressive tumors. Acid pH has been suggested as a key characteristic of aggressive tumors that might distinguish aggressive lesions from more indolent pathology. We therefore investigated the novel class of molecules, pH low insertion peptides (pHLIPs), as markers of low pH in tumor allografts and of malignant lesions in a mouse model of spontaneous breast cancer, BALB/neu-T. pHLIP Variant 3 (Var3) conjugated with fluorescent Alexa546 was shown to insert into tumor spheroids in a sequence-specific manner. Its signal reflected pH in murine tumors. It was induced by carbonic anhydrase IX (CAIX) overexpression and inhibited by acetazolamide (AZA) administration. By using 31P magnetic resonance spectroscopy (MRS), we demonstrated that pHLIP Var3 was retained in tumors of pH equal to or lower than 6.7 but not in tissues of higher pH. In BALB/neu-T mice at different stages of the disease, the fluorescent signal from pHLIP Var3 marked cancerous lesions with a very low false-positive rate. However, only ~60% of the smallest lesions retained a pHLIP Var3 signal, suggesting heterogeneity in pH. Taken together, these results show that pHLIP can identify regions of lower pH, allowing for its development as a theranostic tool for clinical applications.

in vivo fluorescence | carbonic anhydrase IX | pHLIP | invasive tumor | early detection

The reprogramming of metabolism resulting in enhanced glycolysis is now a well-recognized characteristic of many cancers. Increased levels of glycolysis—while contributing to energy generation—are essential to supply carbon backbones for the synthesis of the nucleotides required to sustain DNA synthesis under conditions of abnormal proliferation (1, 2). This, the well-recognized Warburg effect plays a physiological role in sustaining the malignant phenotype. In addition to the requirement for nucleotide synthesis, glycolysis can be essential for energetics under hypoxia. Because a poor vascular supply is also characteristic of cancers, hypoxia generated by poor perfusion is now regarded as a hallmark of cancer (3). This hypoxia, if sufficiently extreme, may dictate that cancer cells as well as macrophages and other stromal cells in the hypoxic microenvironment use glycolysis to maintain bioenergetics. It has recently been established that endothelial cells participating in sprouting angiogenesis rely on glycolysis for their energy requirements (4). Furthermore, many of the most prevalent and well-known oncogenic signaling pathways such as myc and PI3K redirect the cancer cell metabolism toward increased glycolysis (1, 2). Thus, levels of glycolysis greater than those found in normal tissues are associated with malignancy.

One consequence of glycolysis is the production and secretion of lactate, resulting in decreased extracellular pH (5, 6). In addition, cancer cells and especially hypoxic cancer cells express carbonic anhydrases IX and XII (7, 8), which catalyze the formation of extracellular acid from carbon dioxide and thus enhance acidic extracellular pH (9). Extracellular acidity as evoked by tumor progression has the potential to regulate multiple biological processes such as proliferation, angiogenesis, immunosuppression, invasion, and chemoresistance (5, 10–16). Exposure of cancer cell lines to acidic pH (6.8) increased migration and invasion in vitro (17) and in vivo (18). Acidic pH induces increased expression and release of MMP-9 (19) and MMP-2 (18). Reduction of tumor pH by oral bicarbonate treatment reduced metastasis in vivo in xenografts (20). Thus, alterations in extracellular pH are characteristic of cancer and are thought to contribute to aspects of the malignant phenotype and to resistance to some forms of therapy. Cancer rarely arises in a single step but instead represents a series of genetic alterations, eventually leading to fully formed tumors. At the pathological level, this can be seen as lesions first showing hyperproliferation, and dysplasia followed by invasion. This process can be accelerated in mice bearing transgenes that already have genetic alterations that predispose them to cancer. Accordingly, we wished to ask whether detection of acid pH in a tumor might be a useful biomarker for detection of early neoplasia. Because the extracellular pH in tumors is just 0.5–1 pH units lower than the extracellular pH in normal tissue, it has proven challenging to design molecular probes sensitive to this difference. Several magnetic resonance (MR)-based approaches to measure tumor acidity have been developed (21), all with some significant limitations in regards to translation to the clinic. Although a number of pH-sensitive tumor-targeting agents have
been recently introduced (22, 23), the challenge has been to achieve fast pH transition within a single pH unit, to discriminate healthy tissue of normal pH from the more acidic environment of tumors.

A novel class of molecules that target areas of low pH has recently been developed: the pH low insertion peptides (pHLIPs) (24). The mechanism of pHLIP-mediated targeting is based on pH-dependent membrane-associated folding into a coil conformation, which releases free energy (25). This coil inserts into cell membranes and thus allows selective targeting of cancerous tissue of low extracellular pH (pH 6.0–6.8) while avoiding retention in healthy tissue (pH 7.2–7.4). WT-pHLIP has been successfully tested in vitro as an agent for intracellular delivery of large polar cargo molecules (26–29). In addition, WT-pHLIP promotes pH-dependent fusion of pHLIP-coated liposomes containing gramicidin channels with cellular membranes, thus destroying the balance of monovalent ions (30).

In vivo, pHLIP has been used as a marker in mouse models of cancer (31–38), ischemia (39), arthritis (33), and influenza (40). It also has been used to target various nanoparticles (41, 42) (43) and liposomes (39, 44) to acidic tissue. Studies differ as to whether the actual pH was determined by 31P magnetic resonance spectroscopy (MRS) (32, 34, 38) or other methods (45). Tumor pH alteration has been attempted by bicarbonate (34) or carbonic anhydrase IX (CAIX) overexpression (38), and the effect on pHLIP uptake has been registered.

Clinical applications have focused on the topical application of pHLIP, onto biopsies from human head and neck cancer patients, where pHLIP detected cancerous tissue within the samples (46, 47).

However, no systematic assessment of the degree of pHLIP labeling in regard to pathological findings had been undertaken, which is now the main focus of our study. Most of the examples above used WT-pHLIP for their studies. We compared uptake with pHLIP Variant 3 (Var3) and Var7, as these had previously been selected among 16 rationally designed pHLIP variants as the best potential tumor-targeting pHLIPs (24). These data led us to concentrate our efforts on pHLIP Var3, recently introduced as an optimized tumor-targeting pHLIP (24), to correlate its tumor uptake and retention with (i) tumor pH and (ii) manipulation of extracellular pH by CAIX overexpression and inhibition through acetazolamide (AZA) and (iii) evaluate Var3 use under “clinical” conditions for targeting of early and developed lesions using the spontaneous breast cancer model BALB/nu-e−(48) as it progresses from atypical hyperplasia to invasive carcinomas.

**Results**

First we used 4T1 breast cancer cells, which closely mimic triple-negative human breast cancer, grown as allografts in BALB/c mice to assess targeting and retention of fluorescent pHLIPs. pHLIP variants Var3 and Var7 (Table 1) and their corresponding noninserting K-pHLIP controls, all conjugated with Alexa546, were administered by tail vein injection once 4T1 tumors reached 5 mm in geometric mean diameter (GMD; Fig. 1A). Increased fluorescence in the tumors was observed 1 h after injection, with a further increase of the signal over 5 h (Fig. 1 B and C). Fluorescence still persisted after 24 h. pHLIP Var3 had enhanced tumor targeting and greater retention than pHLIP Var7. To account for irregular tumor vasculature as a possible cause for pHLIP retention, we compared pHLIP Var3 and Var7 to their noninserting counterparts K-Var3 and K-Var7 (Table 1). Although injection of the K-pHLIPs led to an increase in fluorescence above background over 24 h (∼250%), fluorescence from pHLIP Var3 and Var7 was 5–10-fold as high, indicating a significant contribution of low pH targeting. Because pHLIP Var3 showed the most persistent fluorescence signal and retention, further experiments were conducted with pHLIP Var3.

Using spheroids as a tissue culture 3D model for tumors, the uptake of pHLIP Var3 and of the K-pHLIP noninserting control peptide was compared between spheroids with different levels of extracellular acidity. We used the cell line HCT116, reported both to have low expression of CAIX and to readily form spheroids (8), and HCT116 transduced to overexpress CAIX, leading to acidification of the extracellular space (8) (Fig. 2A and B). As expected, the CAIX-overexpressing spheroids, generating more acid, grew faster than the empty vector (EV) controls (Fig. S1A) and were targeted by pHLIP Var3 better than EV spheroids. We also compared the K-pHLIP Var3 control with pHLIP Var3 within the same spheroid by tagging them to different fluorochromes (Var3-Alexa546 and K-Var3-Alexa647; Fig. 2C). pHLIP Var3 was detected throughout the spheroid, whereas K-pHLIP Var3 remained on the outside. Thus, the uptake and retention of pHLIP Var3 was sequence-specific and pH-responsive.

Next, we tested whether pHLIP Var3 retention in tumors in vivo was altered by CAIX overexpression (Fig. 3). As reported (8), the growth rate of tumors from CAIX-overexpressing cells (HCT116 CAIX) was greater than that of the controls (HCT116 EV; Fig. 3A). We normalized the fluorescence of pHLIP Var3 to tumor volume. The CAIX-overexpressing tumors (Fig. S1B) had a significantly higher uptake of pHLIP Var3 than the controls at both 5 h and 18 h (Fig. 3B). To establish that pHLIP Var3 uptake by tumors reflected extracellular acid pH, we asked whether inhibition of CAIX activity by AZA (49) would reduce uptake or retention of Var3 within tumors. We injected mice bearing 4T1 tumors with AZA (40 mg/kg, i.p.) followed by injection of pHLIP Var3 24 h later (Fig. 3C). The fluorescence signal from the pHLIP Var3 probe was monitored over another 24 h. The mice treated with AZA showed a significantly greater decline in the fluorescence signal compared with untreated controls. This indicates that pHLIP Var3 retention indeed correlates with the extracellular pH of tumors, that changes in tumor pH will be

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**Table 1. The amino acid sequence of the pHLIP variants and K-pHLIP controls**

<table>
<thead>
<tr>
<th>Probe</th>
<th>Amino acid sequence</th>
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</thead>
<tbody>
<tr>
<td>WT</td>
<td>ACENQPIYWARADYLFTPLPLDALLVDADEGT</td>
</tr>
<tr>
<td>Var3</td>
<td>ACDDQNPWRAYDLPFPLTPDLLDLLW</td>
</tr>
<tr>
<td>Var7</td>
<td>ACEEONPWRAYLWLPFTLLLEL</td>
</tr>
<tr>
<td>K-Var3</td>
<td>ACDDQNPWRAYLWLPFTLLKLLLW</td>
</tr>
<tr>
<td>K-Var7</td>
<td>ACEEONPWRAYLWLPFTLKLLKLL</td>
</tr>
</tbody>
</table>

The transmembrane protonatable D and E (underlined) residues in Var3 and Var7 were replaced by positively-charged K residues (also underlined) in K-Var3 and K-Var7, which prevents K-Var insertion into membrane and thus tumor targeting.
Fig. 2. The ability of pHLIP to penetrate the spheroid is sequence specific. (A and B) Following incubation with fluorescent pHLIP Var3 for 6 h, pHLIP fluorescence in HCT116 spheroids was recorded from equatorial sections in a confocal microscope (magnification, 200×). Within 3 d, the CAIX-overexpressing spheroids (B) grew larger than the EV ones (A). (C) Staining of CAIX-overexpressing spheroids with both Var3 (red) and control peptide K-Var3 (blue) showed that Var3 was retained within the spheroid, whereas K-Var3 was not taken up and remained outside.

Fig. 3. pHLIP uptake and retention is pH dependent. (A) Tumor growth curves of EV and CAIX-overexpressing HCT116 cells in nude mice. CAIX overexpression enhanced tumor growth. (B) The uptake and retention of pHLIP Var3 in CAIX-overexpressing tumors (normalized to volume) was significantly higher than in EV controls over time. (C) AZA treatment reduced pHLIP retention significantly within 24 h. Mice bearing 4T1 tumors were injected with pHLIP and treated with AZA or left untreated. The mice were imaged at 1 h and 24 h postinjection, and the decline in fluorescence was calculated. The increase in pH as effected by AZA accelerated the decrease in pHLIP fluorescence significantly (n = 4–6 per group; data are mean ± SEM).

Discussion
In this study we explored the feasibility of using the pHLIP Var3 peptide as a biomarker for detection of early neoplasia. Our data indicating that pHLIP Var3 exhibits tumor targeting and retention are in good accordance with previous findings with other

reflected by changes in pHLIP Var3 signal, and that protein levels of CAIX do not directly affect pHLIP Var3 retention.

Finally, we attempted to establish a direct correlation of actual pH within the tumor to pHLIP Var3 uptake and retention in vivo. To determine the pH of tumors, we used the 31P MRS method (50). We used inorganic phosphate, phosphocreatine (PCr), and ATP to calculate the overall pH from MRS spectra (Table S1).

According to the literature, approx. 70% of the signal in bulk pH measurement is from intracellular sources and 30% from extracellular ones. Hence, a large enough difference in extracellular pH would still be reflected in the signal (50–52). To avoid contamination of the signals, localized voxels of >125 mm^3 were used rather than global scans, which meant that we could not compare the tumors to normal mammary glands, which are too small in volume. Thus, we compared the pH and pHLIP Var3 fluorescence detected in tumors to muscle (Fig. 4). Although muscle showed an overall pH of 7.1 ± 0.1 (n = 3) and no fluorescence signal above background levels, the pH measured in tumors of the same animal was lower at 6.7 ± 0.0 (n = 3), with a fluorescent signal over background ~5 times higher than in background and 4.2 times higher than in muscle. The measured values represent bulk pH, with the pH at the surface of glycolytic cancer cells expected to be lower (53).

Our data clearly indicate correlations between tissue pH and pHLIP Var3 uptake and retention in vivo, raising questions of whether changes in pH might occur in early neoplasia and whether changes in pH might occur in early neoplasia and whether pHLIP Var3 will be able to reflect these changes. To examine early lesions, we used the transgenic BALB/neu-T model of breast cancer. These mice develop atypical mammary hyperplasia by early lesions, we used the transgenic BALB/neu-T model of breast cancer (48). These mice develop atypical mammary hyperplasia by week 9–10 of age, carcinoma in situ and invasive carcinoma, with an area under the ROC curve of 0.789 ± 0.028 SEM (Fig. 6A and Tables S2 and S3); less so for the presence of necrosis, with an area under the ROC curve of 0.860 ± 0.033 SEM (Fig. 6B and Tables S4 and S5); and less again for the retention of any normal tissue within the tumor, with an area under the ROC curve of 0.789 ± 0.041 SEM (Fig. 6C and Tables S6 and S7). We had wondered whether pHLIP Var3 retention within 24 h. Mice bearing 4T1 tumors were injected with pHLIP and treated with AZA or left untreated. The mice were imaged at 1 h and 24 h postinjection, and the decline in fluorescence was calculated. The increase in pH as effected by AZA accelerated the decrease in pHLIP fluorescence significantly (n = 4–6 per group; data are mean ± SEM).
with its significantly reduced level of $\mu$|\mu|AZA (Sigma) was dissolved in 0.9% sodium chloride/1% DMSO for i.v.
cells were seeded onto
The pH was measured in BALB/neu-T tumors in vivo. To demonstrate
104,000 M
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Mice were used in accordance with the Animals Scientific Procedures
239,000 M
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and
0.0 than the muscle, 7.1 ± 0.0
Spheroids were grown on
pHLIP Var3 detects spontaneously arising tumors in vivo. BALB/neu-T
and
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Tapmeier et al.
Mammography clearly can recognize lesions that are identified
identify disease in patients that affects their long-term survival.
apparent from the disappointing limitations of mammography to
pear to be cancerous by pathological criteria may not actually
Tumor pH may display heterogeneous distribution, affecting the
form progressive lesions. Although these experiments were done
that lesions with more acid pH may be more likely to go on to
Var3 appears to be a good indicator of well-established malig-
and in xenografts by the use of CAIX-positive and -negative
cancer cells leads to differential retention of pHLIP Var3, con-
istent with more acidic extracellular pH. The tuning of pH by
AZA-mediated CAIX inhibition led to a significant decrease in
pHLIP Var3 retention in 4T1 tumors. In previous work we
showed that tumors from a variety of cancer types in mice retain
pHLIP peptides (24, 37, 54). Here we have used both models of
colorectal cancer and breast cancer. Thus, the retention of a
signal from pHLIP Var3 peptide indicates the presence of
extracellular acidosis in murine tumor models, and likely in man.
We then asked whether such a biomarker might be used to
identify early neoplasia. Enhanced utilization of glycolytic me-
tabolism is a characteristic, indeed hallmark, of cancer, however
the time and extent of its induction during carcinogenesis are not
known. Hence we examined the retention of pHLIP Var3 in a
transgenic model of breast cancer. There was no evidence of
retention of pHLIP Var3 in normal breast tissue. These results
indicate that false-positives are uncommon in this model using
pHLIP Var3 as a marker. And all of the larger cancers retained
pHLIP Var3, indicative of acidic pH. Thus, detection of pHLIP
Var3 appears to be a good indicator of well-established malign-
ancy in this model as well. However, although most of the early
lesions retained the pHLIP signal, many did not. This raises the
intriguing possibility that lesions can be stratified based upon
their pHLIP uptake, reflecting the extent of metabolic reprog-
gramming in any given lesion. These results lead to the hypothesis
that lesions with more acid pH may be more likely to go on to
form progressive lesions. Although these experiments were done
using an Alexa Fluor-conjugated version of pHLIP Var3, future
studies in man could use single photon emission computed to-
mography (SPECT) or positron emission tomography (PET)
tracers to enable detection. Fluorescence could possibly be useful
for light imaging of dysplastic lesions of the gastrointestinal tract.
Tumor pH may display heterogeneous distribution, affecting the
overall signal; thus, pH imaging with higher spatial resolution
might be needed to address this potential issue.
It is clear in human breast cancer that many lesions that ap-
appear to be cancerous by pathological criteria may not actually
result in deleterious events for the patient. This is becoming
apparent from the disappointing limitations of mammography to
identify disease in patients that affects their long-term survival.
Mammography clearly can recognize lesions that are identified
by pathology as malignant. However, their removal has only a
limited improvement on long-term survival of the population
overall (55, 56). Our results now raise the question of whether
discrimination of lesional pH might add very valuable predictive
information. Further research to determine whether altered pH
in early neoplastic lesions correlates with biological behavior will
be required and would help to possibly establish pH-based strat-
fication of neoplastic lesions.
In conclusion, we believe that the pHLIPs, in general, and
pHLIP Var3, specifically—with its significantly reduced level of
false-positive signal—have the potential to be predictive markers
of tumor invasiveness and aggressiveness.

Materials and Methods

Synthesis of Fluorescent Constructs. The pHLIP variants were prepared by solid-
phase peptide synthesis using 9-fluorenylmethyloxycarbonyl chemistry and purified
by reverse phase chromatography by James I. Elliott at the W.M. Keck
Foundation Biotechnology Resources Laboratory at Yale University (New
Haven, CT). The concentration of fluorescent pHLIPs was determined by
absorbance using the molar extinction coefficient: $\varepsilon_{\text{556}} = 104,000$ M$^{-1}$ cm$^{-1}$
for Alexa546-pHLIPs and $\varepsilon_{\text{485}} = 239,000$ M$^{-1}$ cm$^{-1}$ for Alexa647-pHLIPs. All
pHLIP peptides (WT, Var3, Var7, K3, and K7) were dissolved in PBS pH 7.4
at a concentration of 40 μM. For in vivo experiments, pHLIP was injected i.v.
(40 μM/100 μL) or otherwise used as indicated.

Cells. All cells were grown in DMEM 10% (vol/vol) FCS with penicillin/
streptomycin at 37 °C, 5% (vol/vol) CO$_2$. The 4T1 cells were from ATCC. The
HCT116 and variants thereof were used as described previously (8).

Fluorescent pHLIP Uptake by Tumor Spheroids. Spheroids were grown on
agarose beds (1%) in tissue culture plates. Briefly, 10$^5$ cells were seeded onto
an agarose bed within a 24-well plate cavity and left to grow for 3 d at 37 °C,
5% (vol/vol) CO$_2$. The resulting spheroid was removed from the cavity and
incubated with pHLIP for 6 h, then washed twice with PBS, and recorded by
z-stack in a confocal microscope (Zeiss 710 LSM).

AZA. AZA (Sigma) was dissolved in 0.9% sodium chloride/1% DMSO for i.v.
injection at 45 mg/kg as described before (49).

Animals. Mice were used in accordance with the Animals Scientific Procedures
Act of 1986 and local ethical guidelines at the University of Oxford following
approval by the local Clinical Medicine Ethical Review Committee. Female
BALB/c mice and BALB/c nude mice were purchased at 8 wk of age from

Fig. 4. The pH was measured in BALB/neu-T tumors in vivo. To demonstrate
the feasibility of in vivo pH measurement, tumor-bearing BALB/neu-T mice
were used in a 9.4T MRI tuned to the $^{31}$P signal. To avoid contamination of the
voxel measured, ISIS was used to specify the area of measurement. No
fluorescence signal above background (FL/BKG) was detected from muscle,
whereas the tumor showed a signal-to-noise ratio of ~2.5. At the same time,
the tumor showed a lower pH of 6.7 ± 0.0 than the muscle, 7.1 ± 0.1 (n = 3 in
both groups; data are mean ± SEM).

Fig. 5. pHLIP Var3 detects spontaneously arising tumors in vivo. BALB/neu-T
mice of different ages and therefore at different stages of tumor de-
development were injected with pHLIP Var3. To measure the fluorescent signal
from the tumors, mice were killed and the mammary glands/tumors were
removed (A). Late stage malignancies were highlighted by marked pHLIP
uptake (c and d), whereas other regions in earlier stages of development in
some cases were marked and in some cases were not marked (a and b). A
total of 164 samples were taken and analyzed. (B) An example of a tumor
showing invasive carcinoma (C) and carcinoma in situ (D).
Charles River. BALB/neu-T mice (48) were bred by the biomedical services unit in Oxford.

In Vivo and Ex Vivo Animal Imaging. For in vivo measurements, animals were anesthetized and placed in an in vivo imaging system (IVIS; Xenogen). Alexa546 fluorescence was read (excitation, 500–550 nm; emission detected between 515 and 650 nm) and compared with a reading of background fluorescence, which was subtracted (Live imaging software V3.2). The result was used to measure region of interest (ROI) fluorescence from the tumors. To visualize mammary glands in BALB/neu-T mice, mice were killed following pHiLP injection, the skin was removed, and tumors imaged in the IVIS. Mammary glands were harvested and one half snap-frozen in liquid nitrogen and the other half fixed in formalin for pathological evaluation.

Histopathology. Formalin-fixed paraffine-embedded samples were cut and stained with H&E. The samples were then graded by a pathologist blind to the experimental groups.

13P MRS Measurement of pH in Vivo. MRS was performed on a 9.4 T 160 mm VNMRS horizontal bore preclinical imaging system equipped with a 100 mm bore gradient insert capable of 400 mT/m (Varian, Inc.). Radio frequency (RF) transmission was performed with an actively decoupled 35 mm ID quadrature birdcage coil (Rapid Biomedical GmbH). RF reception was performed with a custom-made actively decoupled 15 mm surface coil. 13P localization was performed with image-selected in vivo spectroscopy (ISIS) (57) using adiabatic hyperbolic secant inversion pulses with a bandwidth of 15 kHz in combination with outer voxel suppression.


